

Advanced Analyses of Resting-State fMRI (rs-fMRI): PART I

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Download Demo Materials

心智科學腦研究推動網

心智影像研究(MRI)中心 @成大 活動網頁 → 實作資料

http://fmri.ncku.edu.tw/tw/download/20160528_29rsfMRI/adrsfMRIdata.zip

盧家鋒 個人網頁

進階fMRI資料分析理論與實作→ 實作資料

<http://www.ym.edu.tw/~cflu/adrsfMRIdata.zip>

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Course Arrangement



PART I (5/28)

- Preprocessing of rs-fMRI
- SPM preprocessing batch
- Modification of batch file
- Group independent component analysis (group ICA)

PART II (5/29)

- Seed-based functional connectivity
- Complex network analysis

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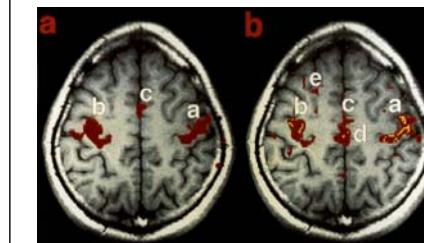
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First rs-fMRI Article (MRM 1995)



Functional Connectivity in the Motor Cortex of Resting Human Brain Using Echo-Planar MRI

Bharat Biswal, F. Zerrin Yetkin, Victor M. Haughton, James S. Hyde



a. Functional activation during tasking
 b. rs-fMRI correlation maps
 (red: positive, yellow: negative)

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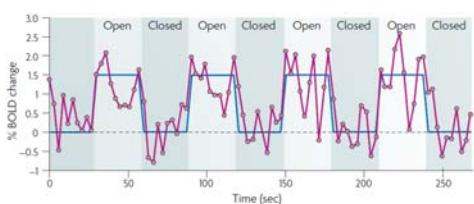
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Spontaneous Fluctuation



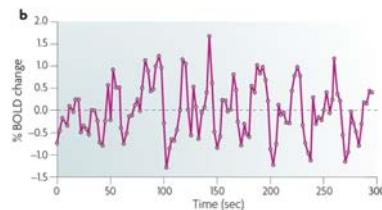
Task-specific fMRI

- ✓ Model-based Analysis
- ✓ Model-free (data-driven) Analysis



Resting-state fMRI (rs-fMRI)

- ✓ Model-free (data-driven) Analysis



Nature Reviews Neuroscience 8.9 (2007): 700-711.

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Employed Software/Package



1. SPM preprocessing

- <http://www.fil.ion.ucl.ac.uk/spm/>

2. REST functional connectivity, ReHo, ALFF, fALFF, VMHC

- <http://restfmri.net/forum/index.php?q=rest>

3. GIFT (v3.0a), group ICA

- <http://mialab.mrn.org/software/gift/#>

4. Brain Connectivity Toolbox/Network Based Statistic Toolbox

- <https://sites.google.com/site/bctnet/>

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Rs-fMRI Analyses



1. Functional connectivity analysis

- Linear correlation analysis
- Independent component analysis (GIFT-ICA; Calhoun et al., NeuroImage 2001)
- Granger causality analysis (GCA), effective connectivity

2. Depicting local features of BOLD signal

http://www.ym.edu.tw/~cflu/CFLU_course_speech.html

- Regional homogeneity (ReHo; Zang et al., NeuroImage 2004)
- Amplitude of low-frequency fluctuation (ALFF; Zang et al., Brain & Development 2007)
- Fractional ALFF (fALFF; Zou et al., J Neurosci Methods 2008)

Functional Integration ⇔ Functional segregation

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Let's Start from Very Beginning



DICOM format!! ⇔ NIfTI (.nii) or Analyze75 (*.hdr, *.img)

REST > data > dicom > Subj01 > REST

Name

- MR.HEAD_IBRU.3.1.2011.02.21.12.20.42.328125.100216930.IMA
- MR.HEAD_IBRU.3.2.2011.02.21.12.20.42.328125.100216948.IMA
- MR.HEAD_IBRU.3.3.2011.02.21.12.20.42.328125.100216966.IMA
- MR.HEAD_IBRU.3.4.2011.02.21.12.20.42.328125.100216984.IMA
- MR.HEAD_IBRU.3.5.2011.02.21.12.20.42.328125.100217002.IMA
- MR.HEAD_IBRU.3.6.2011.02.21.12.20.42.328125.100217020.IMA
- MR.HEAD_IBRU.3.7.2011.02.21.12.20.42.328125.100217038.IMA

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DICOM (1993)

- Digital Imaging and Communication in Medicine



NEMA, Suite 1752
1300 North 17th Street
Reston, VA 22090
Ph: (703) 841-3285
<http://dicom.nema.org/>



- ACR & NEMA formed a committee in 1983
 - American College of Radiology
 - National Electrical Manufacturers Association

"The Common Language of Medical Equipment"

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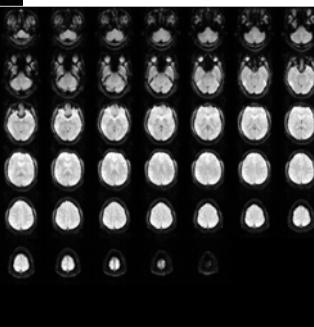
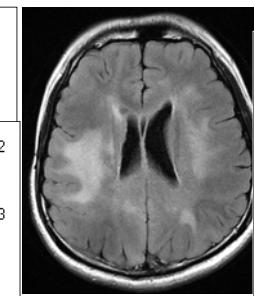
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DICOM format

Header

```
0008,0020,Study Date=20151204
0008,0021,Series Date=20151204
0008,0022,Aquisition Date=20151204
0008,0023,Image Date=20151204
0008,0030,Study Time=122630
0008,0031,Series Time=122800
0008,0032,Aquisition Time=122800
0008,0033,Imag[0018,0050],Slice Thickness=5
0008,0050,Acc[0018,0080],Repetition Time [TR, ms]=8002
0008,0060,Mod[0018,0081],Echo Time [TE, ms]=127.948
0008,0070,Mar[0018,0082],Inversion Time=2000
0008,0080,Inst[0018,0083],Number of Averages=1
0008,0090,Ref[0018,0084],Imaging Frequency=63.854903
0008,1010,Stat[0018,0085],Imaged Nucleus=1H
0008,1030,Stu[0018,0086],Echo Number=
0008,1036,Seq[0018,0087],Magnetic Field Strength=1.5
0008,1070,Dop[0018,0088],Spacing Between Slices=6
0008,1090,Mar[0018,0091],Echo Train Length=1
```

Retrieve of subject/imaging information.
Use with caution! Personal privacy!



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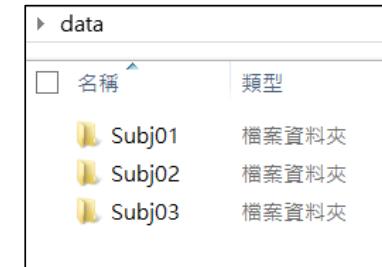
<HTTP://WWW.YM.EDU.TW/~CFLU>

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Switch current folder to data folder

More convenient to execute the subsequent processing steps....

Current Folder: <C:\Users\Alvin\Desktop\data\data\Subj01>



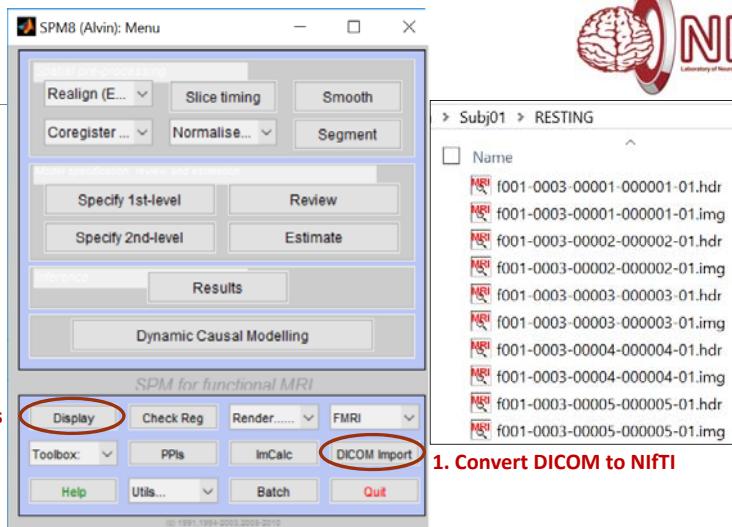
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<HTTP://WWW.YM.EDU.TW/~CFLU>

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DICOM import

2. Check converted images



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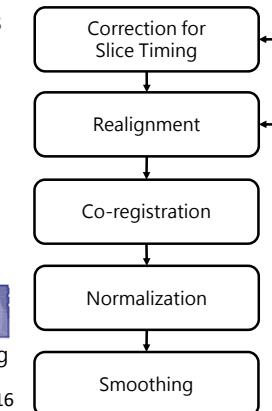
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Preprocessing for rs-fMRI



Similar to that used for task-specific fMRI analysis

- Slice timing
- Realignment
- Co-registration (with anatomical images)
- Normalization
- Smoothing
- Segment (tissue classification; optional)



Standard procedure for fMRI preprocessing

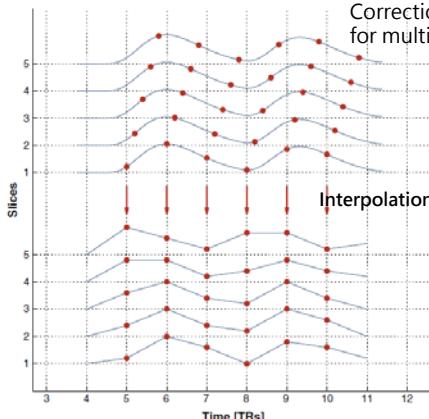
http://www.ym.edu.tw/~cflu/CFLu_course_mriprin.html, Week 16

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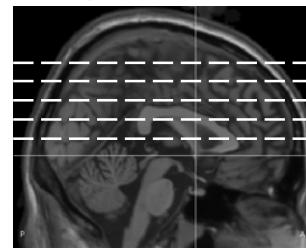
Correction for Slice Timing



Correction for slightly different imaging timing for multi-slice acquisition in a TR.



For example:
Acquire 5 slices in 1 TR
→ Temporal offset between slices



Sladky et al, NeuroImage 2011, 58:588-594.

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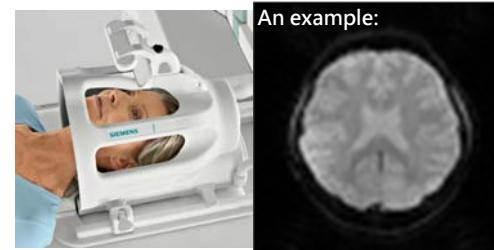
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Realignment of head motion

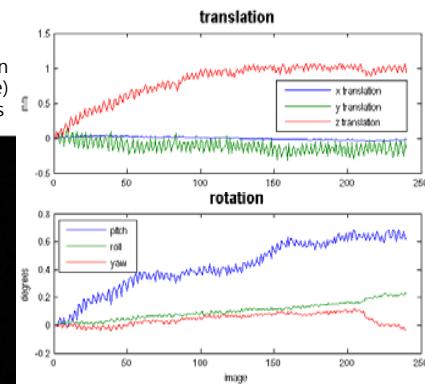


The signal variation from movement is larger than hemodynamic response.

6-parameter Rigid body registration & transformation (align to the 1st volume)
→ 6 co-variates for rs-fMRI analysis



An example:

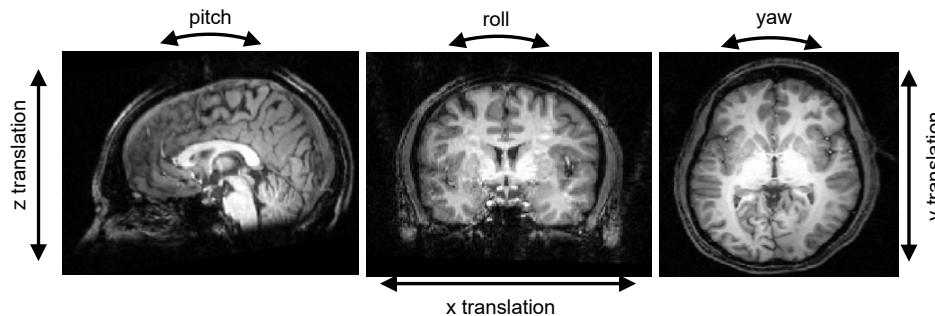


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3 translations and 3 rotations



fMRI slides from <http://culhamlab.ssc.uwo.ca/fmri4newbies/Tutorials.html>

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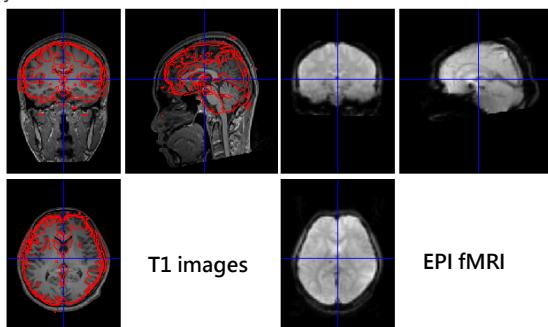
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Co-registration



Align fMRI (EPI) data to structural (T1) images.

- Rigid body transformation using mutual information
- Manual adjustment



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EPI undistortion/unwarp



Magnetic inhomogeneity can cause

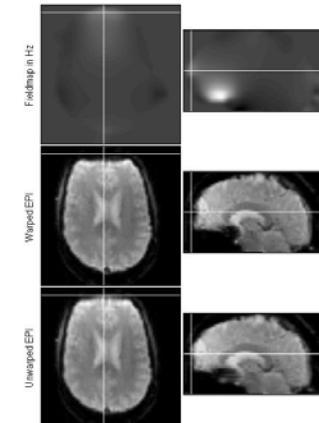
- Signal loss
- Spatial distortion

Magnetic field warps at tissue boundaries

- The frontal pole, orbito-frontal cortex
- Medial temporal lobe (hippocampus)

The benefit of undistortion/unwarp

- Make the shape of an individual's fMRI data more similar to their anatomical images.



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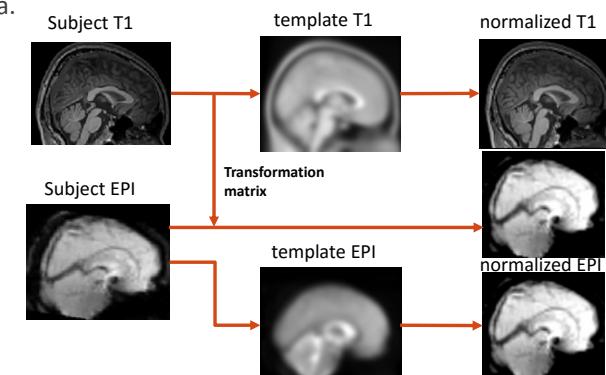
[HTTP://WWW.YM.EDU.TW/~CFLU](http://WWW.YM.EDU.TW/~CFLU)

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Normalization



We can perform spatial normalization using either anatomical (T1) images or fMRI (EPI) data.



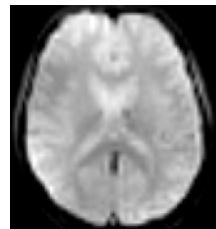
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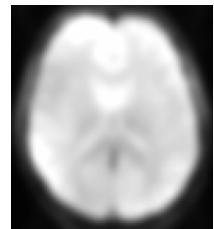
Gaussian Smoothing

- Each voxel becomes weighted average of surrounding voxels.
- Render the data more normally distributed.
- Compensate for inaccuracies in normalization between individuals.
- Increase signal-to-noise ratio



$2 \times 2 \times 2 \text{ mm}^3$

normalization



Normalization+smoothing

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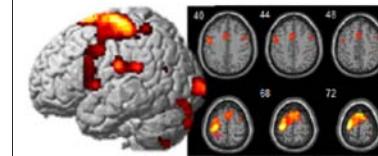
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Preprocessing Step-by-step

fMRIprocess_CFLu.pdf

http://www.ym.edu.tw/~cflu 6/11/2014 Lesson 16 Chia-Feng Lu
國立陽明大學 物理治療暨輔助科技學系
盧家鋐 助理教授

功能性磁振影像分析



http://www.ym.edu.tw/~cflu/MRI_PrinApp_Class16_CFLu.pdf

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三、使用 SPM

1. 開啟 MATLAB (請確認已完成 Set Path)，在 command window 鍵入 spm fmri
2. 依序練習執行 (請使用 dataset_L16/Subj01 中的影像)
 - (1) Slice timing : 校正不同切面取樣時間的差異 (Siemens MRI 之 interleave images，如為偶數張切面取樣順序為 2, 4,..., 1, 3,...；奇數張切面順序為 1, 3,..., 2, 4,...)
 - (2) Realign (Est & Res) : 校正不同 volume 間的頭部移動
 - (3) Coregister (Estimate) : 將 T1 影像對位至 fMRI 影像 (使用 Check Reg 檢查對位結果)
 - (4) Segment : 計算 GM、WM 與 CSF 的機率圖形
 - (5) Normalise : 將影像標準化至 ICBM-152 模板 (Bounding box: -100 -130 -80; 100 100 110)
 - (4) Smooth : 對 fMRI 影像進行三維高斯平滑化處理

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Batch Step-by-step

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➤ 輸入基本參數(dataset_L16\fMRIbatch_process.mat)
請按照以下步驟依序設定各 module 的參數

- ✓ Named Directory Selector : Input Name 填入 subject directory；在 Directories 中點兩下讓 Directory 出現一個<-X 的標記
- ✓ Make Directory : New Directory Name 輸入 stats，提供 SPM 統計分析擺放檔案的位置
- ✓ Slice Timing : Data 點兩下出現<-X；Number of Slices: 40; TR:2; TA 輸入 2-(2/40); Slice order:[2:2:40,1:2:40]; Reference Slice:1
- ✓ Realign : Data 點兩下，讓 Session 出現<-X
- ✓ Normalise : Data 點兩下加入一個 Subject；更改 bounding box 為 -100 -130 -80; 100 100 110
- ✓ Smooth : 可調整 FWHM 參數

五、附錄：Batch 檔設定詳細說明

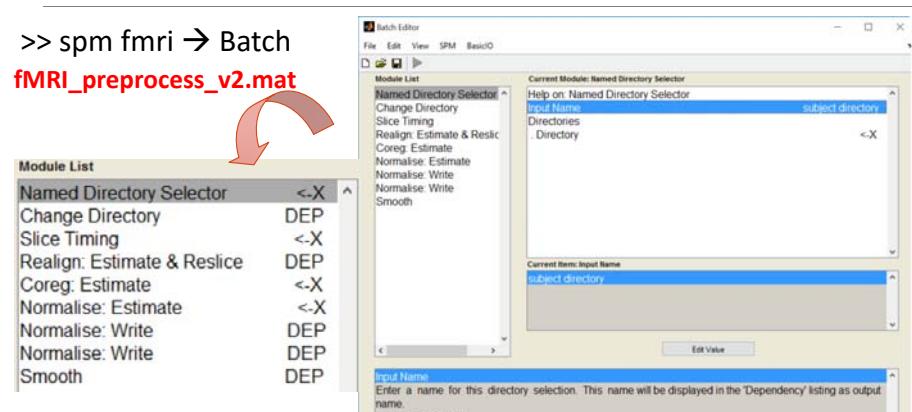
- 建立基本處理流程(dataset_L16\fMRIbatch_raw.mat)
1. 請先將下列順序的 module 加入至 batch 中
 - ✓ BasicIO -> Named Directory Selector
 - ✓ BasicIO -> Change Directory
 - ✓ BasicIO -> Make Directory
 - ✓ SPM -> Temporal -> Slice Timing
 - ✓ SPM -> Spatial -> Realign: Estimate & Reslice
 - ✓ SPM -> Spatial -> Coreg: Estimate
 - ✓ SPM -> Spatial -> Segmentation
 - ✓ SPM -> Spatial -> Normalise: Write
 - ✓ SPM -> Spatial -> Smooth

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>> spm fmri → Batch
fMRI_preprocess_v2.mat



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Batch of SPM fMRI preprocessing



>> spm fmri

Save as your own batch template

Module List

Named Directory Selector	<-X
Change Directory	DEP
Slice Timing	<-X
Realign: Estimate & Reslice	DEP
Coreg: Estimate	<-X
Normalise: Estimate	<-X
Normalise: Write	DEP
Normalise: Write	DEP
Smooth	DEP

T1 template image
C:\Users\Alvin\Desktop\softwares\spm8\templates\T1.nii,1

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Batch of SPM fMRI preprocessing



>> spm fmri

Save as subject's batch

Module List

Named Directory Selector	<-X
Change Directory	DEP
Slice Timing	<-X
Realign: Estimate & Reslice	DEP
Coreg: Estimate	<-X
Normalise: Estimate	<-X
Normalise: Write	DEP
Normalise: Write	DEP
Smooth	DEP

Subject data folder
C:\Users\Alvin\Desktop\data\data\Subj01

rs-fMRI data
C:\Users\Alvin\Desktop\data\data\Subj01\REST.img,1
...
C:\Users\Alvin\Desktop\data\data\Subj01\REST.img,240
240 volumes

T1W data
C:\Users\Alvin\Desktop\data\data\Subj01\anat.img,1

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HTTP://WWW.YM.EDU.TW/~CFLU

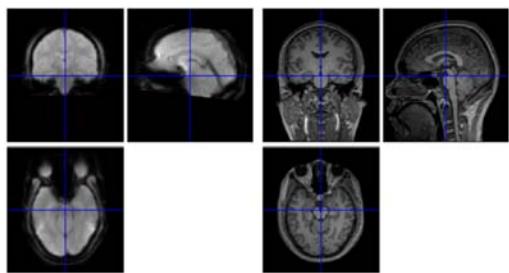
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Always Check Your Data!



SPM processing logfile (spm_2016May28.ps)

<https://online2pdf.com/convert-ps-to-pdf>



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HTTP://WWW.YM.EDU.TW/~CFLU

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Modification of Batch File



Batch Editor → View → Show .m Code

```
Batch Code Browser
matlabbatch(1).cfg_basicio.cfg_named_dir.name = 'subject_directory';
matlabbatch(1).cfg_basicio.cfg_named_dir.dirs = {'C:\Users\Alvin\Desktop\data_proc\Subj02\'};
matlabbatch(2).cfg_basicio.cfg_cd.dir(1) = cfg_dep;
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).tname = 'Directory';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).tgt_spec(1)(1).name = 'filter';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).tgt_spec(1)(1).value = 'dir';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).tgt_spec(1)(2).name = 'strtype';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).tgt_spec(1)(2).value = 'e';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).aname = 'Named Directory Selector: subject_directory(1)';
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).src_exbranch = substruct('.', 'val', '{}', '{}', '.', 'val', '{}', '{}');
matlabbatch(2).cfg_basicio.cfg_cd.dir(1).src_output = substruct('.', 'dirs', '{}', '{}');
%%
matlabbatch(3).spm.temporal.st.scans = {
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00001-00001-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00002-00002-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00003-00003-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00004-00004-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00005-00005-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00006-00006-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00007-00007-
    'C:\Users\Alvin\Desktop\data_proc\Subj02\RESTING\f002-0004-00008-00008-
```

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Independent Component Analysis



A cocktail-party problem



Number of microphones >= number of speakers

$$\begin{aligned}x_1(t) &= 0.7s_1(t) + 0.2s_2(t) + 0.1s_3(t) \\x_2(t) &= 0.3s_1(t) + 0.4s_2(t) + 0.3s_3(t) \\x_3(t) &= 0.1s_1(t) + 0.2s_2(t) + 0.7s_3(t)\end{aligned}$$

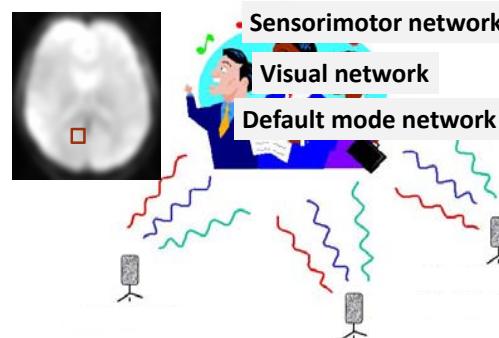
$$\begin{bmatrix} x_1(t) \\ x_2(t) \\ \vdots \\ x_m(t) \end{bmatrix} = \mathbf{A} \begin{bmatrix} s_1(t) \\ s_2(t) \\ \vdots \\ s_k(t) \end{bmatrix}$$

\mathbf{A} is the mixing matrix

Independent Component Analysis



A cocktail-party problem



Number of microphones >= number of speakers

$$\begin{aligned}x_1(t) &= 0.7s_1(t) + 0.2s_2(t) + 0.1s_3(t) \\x_2(t) &= 0.3s_1(t) + 0.4s_2(t) + 0.3s_3(t) \\x_3(t) &= 0.1s_1(t) + 0.2s_2(t) + 0.7s_3(t)\end{aligned}$$

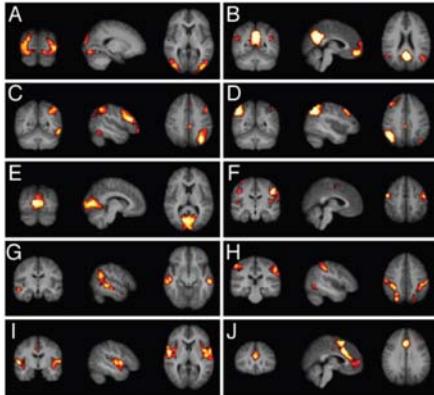
$$\begin{bmatrix} x_1(t) \\ x_2(t) \\ \vdots \\ x_m(t) \end{bmatrix} = \mathbf{A} \begin{bmatrix} s_1(t) \\ s_2(t) \\ \vdots \\ s_k(t) \end{bmatrix}$$

\mathbf{A} is the mixing matrix

Independent components

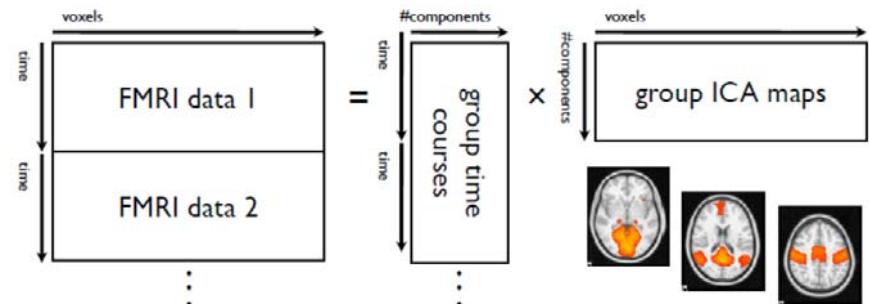


- A. parts of visual cortex
- B. default mode network
- C & D. left and right memory function
- E. visual cortex
- F. sensorimotor cortex
- G. occipitotemporal pathway (ventral stream)
- H. superior parietal cortex
- I. auditory cortex
- J. executive control & working memory



Consistent resting-state networks across healthy subjects. PNAS 2006, 103(37): 13848-13853.

Group ICA/ Concat-ICA

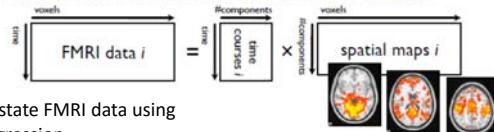


Group comparison of resting-state FMRI data using multi-subject ICA and dual regression

Dual Regression

Dual Regression: This is used to identify, within each of the N individual subjects' FMRI data, spatial maps and associated timecourses corresponding to the multi-subject ICA components. For each individual dataset separately:

- (A) use the group-level spatial maps as a set of spatial regressors in a GLM, to find temporal dynamics associated with each group-level map
- (B) normalization of these timecourses to unit variance (optional, depending on what question the experimenter wants to ask later)
- (C) use these timecourses as a set of temporal regressors in a GLM, to find subject specific maps (still associated with the group-level spatial maps):



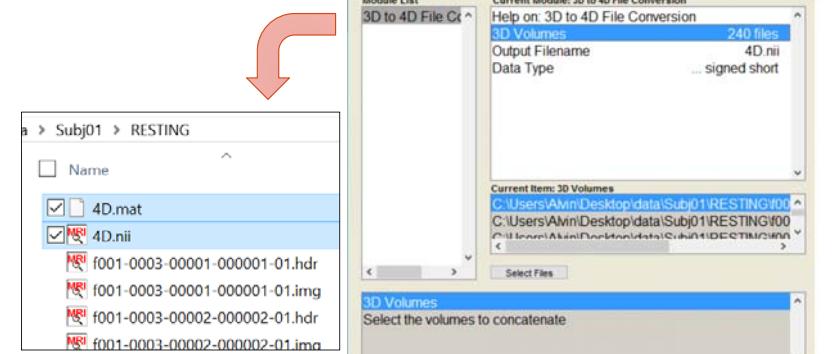
Group comparison of resting-state FMRI data using multi-subject ICA and dual regression

Q & A

THE END
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3D to 4D File Conversion

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